Pneumatic capillary gun for ballistic delivery of microparticles

Dmitry Rinberg
Monell Chemical Senses Center, 3500 Market Street, Philadelphia, Pennsylvania 19104

Claire Simonnet and Alex Groisman
Department of Physics, University of California, San Diego, 9500 Gilman Drive, La Jolla, California 92037

(Received 9 March 2005; accepted 15 May 2005; published online 29 June 2005)

A pneumatic gun for ballistic delivery of microparticles to soft targets is proposed and demonstrated. The particles are accelerated by a high-speed flow of helium in a capillary tube. Vacuum suction applied to a concentric larger diameter tube is used to divert substantially all of the flow of helium from the gun nozzle, thereby preventing the gas from hitting and damaging the target. Speed of ejection of micron-sized gold particles from the gun nozzle, and their depth of penetration into agarose gels are reported. © 2005 American Institute of Physics. [DOI: 10.1063/1.1951044]

High-density micron-size particles accelerated to high speeds can penetrate deep inside live tissues without inflicting much damage to the cells and have been used to effectively deliver genetic material. This method of ballistic delivery is often called “biolistics” and the device for shooting particles—“gene gun”. Biolistics proved to be an efficient method for delivery of plasmids and transfection of prokaryotic and eukaryotic (including mammalian) cells. Most recently it has been used to stain neuronal tissue with fluorescent dyes.

A hand-held commercially available version of the gene gun, Helios™ by BioRad (Hercules, CA), uses ~1 μm in diameter particles made of gold or tungsten, which are accelerated by a short pulse of a high-speed flow of helium (He). Although the carrier particle size has been selected to minimize the cell injury, the high-speed jet of He emerging from the gun nozzle can produce severe damage to soft tissue. In order to slow the flow of He, the nozzle expands toward the end, the target is usually shot from a significant distance, and sometimes a mesh filter is placed between the nozzle and the target. Although there is little data on the actual speeds of the particles launched from the Helios gene gun, all of those measures result in deceleration of the particles and reduction of their penetration depth. A major increase in the depth of penetration into an agarose gel (used to emulate a brain tissue) was reported with a more focused jet of He and short shooting distance, but there was a concomitant increase in damage of the gel surface. A large penetration depth with minimal damage would be very beneficial for staining and transfection of a variety of live tissues, in particular, mammalian brain where most of the cell bodies lie 100 μm below the surface.

In this letter, we propose an alternative design of a pneumatic gun for ballistic particle delivery. Its key feature is the use of active vacuum suction to completely divert the high-speed flow of the gas (He) from the gun nozzle, so that there is no damage to the target from the gas flow (Fig. 1). The particles are accelerated by continuous high-speed flow of He in the inner capillary tube (ICT). The suction is continuously applied through the outer capillary tube (OCT). The diversion occurs over a distance of less than 1 mm, on a time scale of ~2 μs and is expected to have a minimal effect on motion of the particles, which have more inertia than the He gas.

ICT is made of polyamide-coated fused silica (Micro-Fil™ Gauge 23, WPI Inc., Sarasota FL), has an inner diameter D1 = 530 μm and outer diameter 665 μm, and is glued to a plastic luer adapter [Fig. 1(a)]. OCT is a piece of stainless-steel tube with inner and outer diameters of 1.70 and 2.11 mm, respectively. It is made concentric with ICT by two 150 μm thick “gears” [Fig. 1(b)]. The end of ICT is covered by a 0.2 mm circular cap with a 150 μm opening in the middle. The cap is 50 μm thick and has three 100 μm tall pillars for mechanical strength and self-centering with OCT, to which it is glued [Fig. 1(b)]. The cap and the gears are micromachined out of UV-curable epoxy SU8 (MicroChem, Newton MA) using contact lithography. The opening in the cap, ICT and OCT are coaxial within ∼25 μm. OCT is connected to a vacuum through an ~1.5 mm opening in its side at ∼20 mm from the cap. We empirically found that the best results are achieved, when the distance between the cap and the end of ICT is in the range of 600–900 μm. Four individual guns with distances in that range were tested, and their performance was virtually indistinguishable. The lengths of ICT, L1, were 50–55 mm.

![Fig. 1. (Color online) Schematic drawings showing: (a) design and operation of the capillary gun, (b) micromachined concentric gear and end cap; and (c) connection of the gun to pressurized He and vacuum system.](image_url)
The gun was mounted vertically with the cap facing down and was connected to a vacuum system with a gauge pressure $P_o = -86 \text{kPa}$ [Fig. 1(c)]. The ICT inlet was connected to an adjustable pressure source of compressed He. The He pressure was set at $P = 120 \text{kPa}$, 2–3% below the point where a directed stream of He emerging from the cap could be detected by appearance of ripples on the surface of water $\sim 1 \text{ mm}$ under the cap. In order to estimate the average speed of flow at the outlet of ICT, $\bar{v}_o$, we put a gas flow meter (Cole-Parmer, EW-03267-22) upstream from the gun. It was calibrated to display the volumetric flow rate, $Q$, corresponding to the volume of He at atmospheric pressure, and $\bar{v}_o$ was calculated as $Q/(\pi D_i^2/4) \approx 660 \text{ m/s}$. (With the vacuum suction disconnected and the cap removed, $Q$ dropped by only 5%, suggesting that the pressure at the outlet of ICT was close to atmospheric.) The impact of the flow onto the water surface was less than that of a flow through ICT at 0.2 m/s without the vacuum suction. Therefore, substantially all of the flow of He was diverted to the vacuum system.

In order to inject particles into the flow, the ICT inlet was connected to the compressed He through two parallel lines of thick flexible tubing [Fig. 1(c)]. The first line was always open, while the second line was normally kept closed by a solenoid valve. The particles were loaded as a dry powder into a short detachable segment of tubing in the second line downstream from the solenoid valve [Fig. 1(c)]. They were “fired” by opening the valve for 300 ms, thus creating a flow of He that introduced the particles into ICT.

To characterize the performance of the gun, we made test shots into agarose gels, which are commonly used to emulate live tissues. We used three types of spherical gold particles (BioRad) that we call A, B, and C, with respective diameters, $d$, of $0.47 \pm 0.15$, $1.1 \pm 0.1$, and $1.27 \pm 0.27 \text{ m}$m. The size distributions in the particle samples were characterized under an electron microscope. The gels were inspected under dark-field illumination with a $50 \times /0.5$ objective. Representative photographs of a 3% gel, which was imaged at various depths upon shooting with B particles from a distance of 1 mm, are shown in Figs. 2(a)–2(c). The particles near the plane of image are seen as sharp bright dots, while the out-of-focus particles contribute to the bright background. The particles are spread over a circle of $\sim 150 \text{ m}$m in diameter, which closely matches the opening in the cap. For comparison, if the sample was with a Helios gun from $\sim 4 \text{ cm}$ at an intermediate 175 psi pressure setting [Figs. 2(d)–2(f)]. The particles covered a total area $\sim 1.2 \text{ cm}$ in diameter.

It is apparent from the images in Fig. 2 that unlike the Helios gun, the capillary gun delivers very few particles to the surface and a notably larger number of particles to $55 \mu m$ than to $35 \mu m$ depth. The number of particles at different depths, $z$, was counted by taking a stack of images with a step of $3 \mu m$ in depth and using Image-Pro software (Media Cybernetics, Silver Spring, MD) to identify bright dots. The distributions of the three kinds of particles by $z$ for shots with the capillary gun and Helios gun at 175 and 120 psi are shown in Fig. 3. (The latter pressure is preferable for staining delicate brain tissue.) Each curve represents statistics on $\sim 10^4$ individual particles. With the capillary gun, the mean $z$ for particles A, B, and C are 20, 39, and 38 $\mu m$, respectively. With the Helios gene gun, the mean $z$ are 17, 36, and 39 $\mu m$ and 4.5, 32, and 48 $\mu m$ at 175 psi and 120 psi, respectively. Thus, penetration depths with the capillary gun are consistently larger for small particles, especially when it is important to minimize the impact of the gas jet on the target. Further, while the depth distributions for the Helios gun are very broad, the distributions for the capillary gun have characteristic peaks at depths $z_p$ near the maximal penetration depths (Fig. 3). The peak is narrowest for the most monodisperse sample B, where about 60% of the particles are found at $z$ between 40 and 80 $\mu m$.

The particles were ballistically delivered using the capillary gun into 0.25–3% agarose gels with no apparent damage to the gel surface other than particle perforation. As expected, mean $z$ decreased with both shooting distance and agarose concentration, due to viscous friction in air and higher resistance to particle motion in denser gels. However, in all cases the distributions of $z$ had the distinct peak near the maximal penetration depth (cf. Fig. 3), and we assumed it to be a counterpart of a peak in velocity distribution of particles reaching the gel surface.

To estimate the velocity at that peak, $u_p$, we made shots into a 0.25% gel (where the depth of penetration was maxi-
mal) in an atmosphere of hydrogen (H$_2$) from various distances, $h$, between the cap and the gel surface, and plotted $z_p$ as a function of $h$ (inset in Fig. 3). We chose H$_2$ because of its high speed of sound, $v_s$ $\approx$ 1300 m/s, and high kinematic viscosity, $\eta_H/\rho_H$ $\approx$ 1.1 $\times$ 10$^{-4}$ m$^2$/s, which reduce nonlinearity in particle flow resistance associated with finite Mach number, $M$ = $u/v_s$, and Reynolds number, $Re = u \rho_H/\eta_H$, respectively. (Here $u$ is the particle velocity). In addition, the viscosity of H$_2$, $\eta_H$ = 9 $\times$ 10$^{-6}$ Pa s, is half the viscosities of air and He. That expands the range of $h$ and improves resolution of the measurements. The dependencies of $z_p$ on $h$ are close to a linear decay for all three kinds of particles (inset in Fig. 3).

The condition $z_p$ = 0 is met at distances $h_0$ = 22, 44, and 70 mm for particles A, B, and C, respectively (inset in Fig. 3). We can estimate velocity at the peak of the distribution for particles emerging from the gun, $u_0$, if we assume that $z_p$ = 0 corresponds to $u_0$ = 0. Assuming that the corrections due to finite M are small, the flow resistance experienced by the particles can be estimated as $F = -3\pi k d \eta_H [1 + 0.15(kRe)^{0.69}]$. Here $k = (1 + 4.5Kn)^{-1}$ is a correction factor to the Stokes resistance due to finite Knudsen number, Kn = $\lambda/d$, where $\lambda$ = 0.125 $\mu$m is the mean-free path of the H$_2$ molecules. We use the equation of motion, $F = \rho g$ $\pi d^2 u$, (where $\rho_g$ = 1.93 $\times$ 10$^4$ kg/m$^3$ is the density of gold) to obtain a differential equation for $u$, and integrate it numerically to obtain $h_0$ as a function of $u_0$ for various $d$. The values of $u_0$ calculated this way for $h_0$ and mean $d$ of particles A, B, and C are 400, 230, and 280 m/s, respectively (with estimated errors of about 15%). For H$_2$ atmosphere, those values suggest $M$ < 0.3 and less than 1% addition to the resistance due to finite M for all particle sizes, in agreement with the assumption made.

It is instructive to compare the speeds of the particles with characteristic speeds of flow in ICT. The average flow speed at the ICT outlet is $\bar{v}_o$ $\approx$ 660 m/s, but it is significantly lower upstream from the outlet because of compressibility of He. At the ICT inlet, where the absolute pressure is about 2.2 atm, the average speed of He is estimated as $\bar{v}_i$ = $\bar{v}_o$/$\sqrt{2}$. $\phi_a$ = 290 m/s. Thus, although the speeds of the particles are significantly lower than $\bar{v}_o$, they are comparable with $\bar{v}_i$. This result appears reasonable in view of large characteristic length, $L_a$, required for acceleration of the particles to the high speeds of flow in ICT. The length can be estimated as $L_a = \sqrt{2F/m} = \rho_d u_d^2/18k \eta_h [1 + 0.15(kRe)^{0.69}]$ (Here We = $ud\rho_d/\eta_h$, with $\rho_d$ = 0.165 kg/m$^3$ and $\eta_h$ = 2.10$^{-3}$ Pa s, and $k$ is calculated with $\lambda$ = 0.2 $\mu$m for He molecules). With $v$ = $\bar{v}_o$ for particles B and C is 55 and 67 mm, respectively, which is comparable to the length of ICT, $L_i$. For particles A, we obtain a relatively short $L_a$ of about 19 mm, which is a probable reason for their higher characteristic speed.

Increasing $L_i$, while keeping $\bar{v}_o$ the same, requires higher driving pressures, which imply proportionally lower $\bar{v}_i$. Thus, guns with longer ICT that we tested did not give an appreciable increase in the particle penetration depths. However, the depths significantly increased when $D_i$ was expanded from 250 to 530 $\mu$m, allowing lower driving pressure. The expansion of ICT may also have reduced negative effects of uncontrolled transverse motion of the particles and inelastic collisions with the walls. Those collisions may be a cause of the wide distributions of the particle penetration depths (Fig. 3). Further expansion of ICT proved impractical, though, since it caused a reduction of the velocity of the fastest flow which could be diverted to OCT.

The proposed capillary gun is an easily fabricated alternative to Helios gun. In a pilot experiment, we shot B particles coated with a reporter plasmid expressing green fluorescent protein (gWIZ; Aldevron, Fargo, ND) into 293T/17 cells obtained from American Type Culture Collection. After 4 h fluorescence expressed GFP was observed in a number of cells. The capillary gun gives large penetration depths for small particles without damaging the surfaces of even the most delicate targets (0.25% agarose gels). It selectively targets small areas and can be inserted into openings down to 2.5 mm in size. So, it may find applications in medicine and live animal biology. A large fraction of the particles is delivered to a narrow interval of depths, and the characteristic penetration depth is reliably controlled by tailoring the shooting distance. The possibility to estimate and control the speed of the particles makes the gun a promising tool to study microscopic mechanical properties of soft materials.

The authors are very grateful to David Schultz and Jim Glass from Seashell LLC for multiple useful discussions, encouragement, and help with the measurements.

---